

# Decomposition of Skin Color Image

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# Outline

- Objective
- Overview
- Optics of human skin
- Different decomposition methods of skin color image
- Experimental results and evaluation
- Conclusion and perspective



# Objective

*In-vivo* studies in dermatology and cosmetic science need to quantify skin color, erythema or pigmentation objectively and can be relevant for melanoma diagnostic.





# Overview

## Imaging based methods include:

- RGB imaging (digital color image)
  - Absorbance spectra based method [H. Takiwaki, 2008]
  - HSV color model based method [D. H. Kim, 2006]
  - PCA and ICA based method [N. Tsumura, 1999]
- Multi-spectral imaging



# Optics of human skin

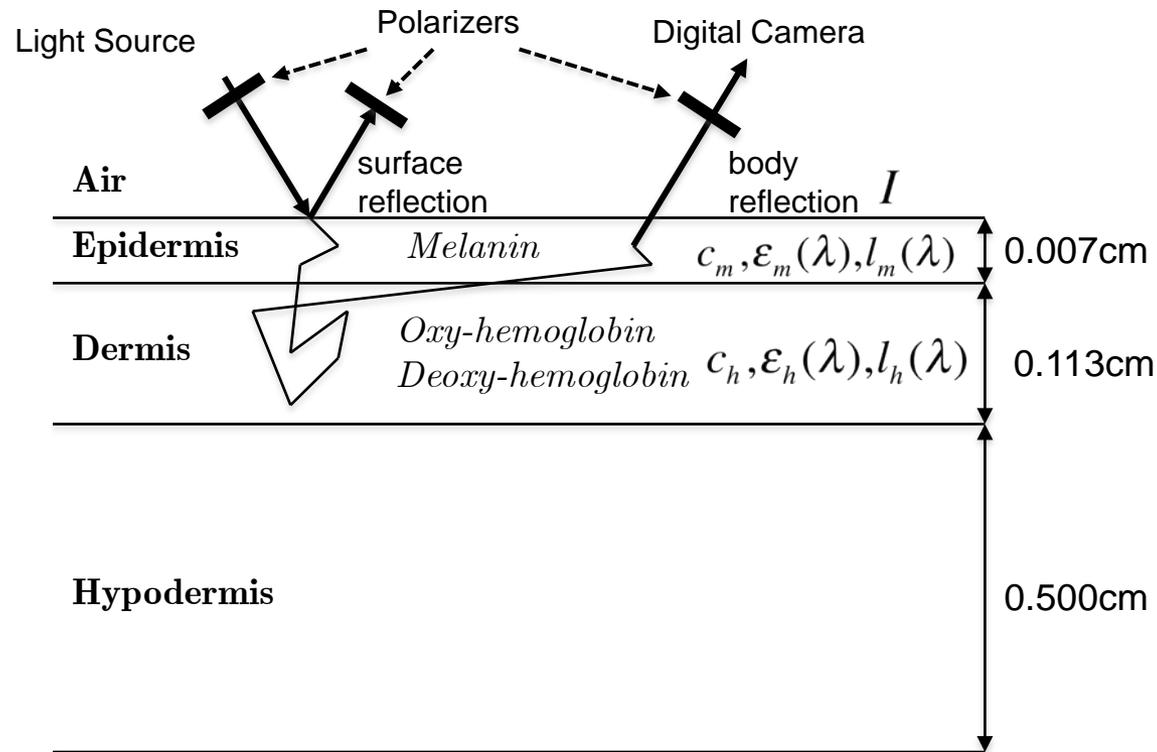


Fig.1. Schematic model of imaging process of three layered model of skin



# Optics of human skin

Based on *Beer-Lambert law*, the absorbance  $A_\lambda$  of this skin model at a wavelength  $\lambda$  is expressed as

$$A_\lambda = \log(1 / R_\lambda) = M_\lambda C_m + H_\lambda C_h + D \quad (1)$$

where  $R_\lambda$  is the reflectance of the skin

$M_\lambda$  and  $H_\lambda$  are coefficients depend on absorbance spectra of melanin and hemoglobin

$C_m$  and  $C_h$  represent respective amounts of melanin and hemoglobin

$D$  is apparent absorbance of the dermis



# Optics of human skin

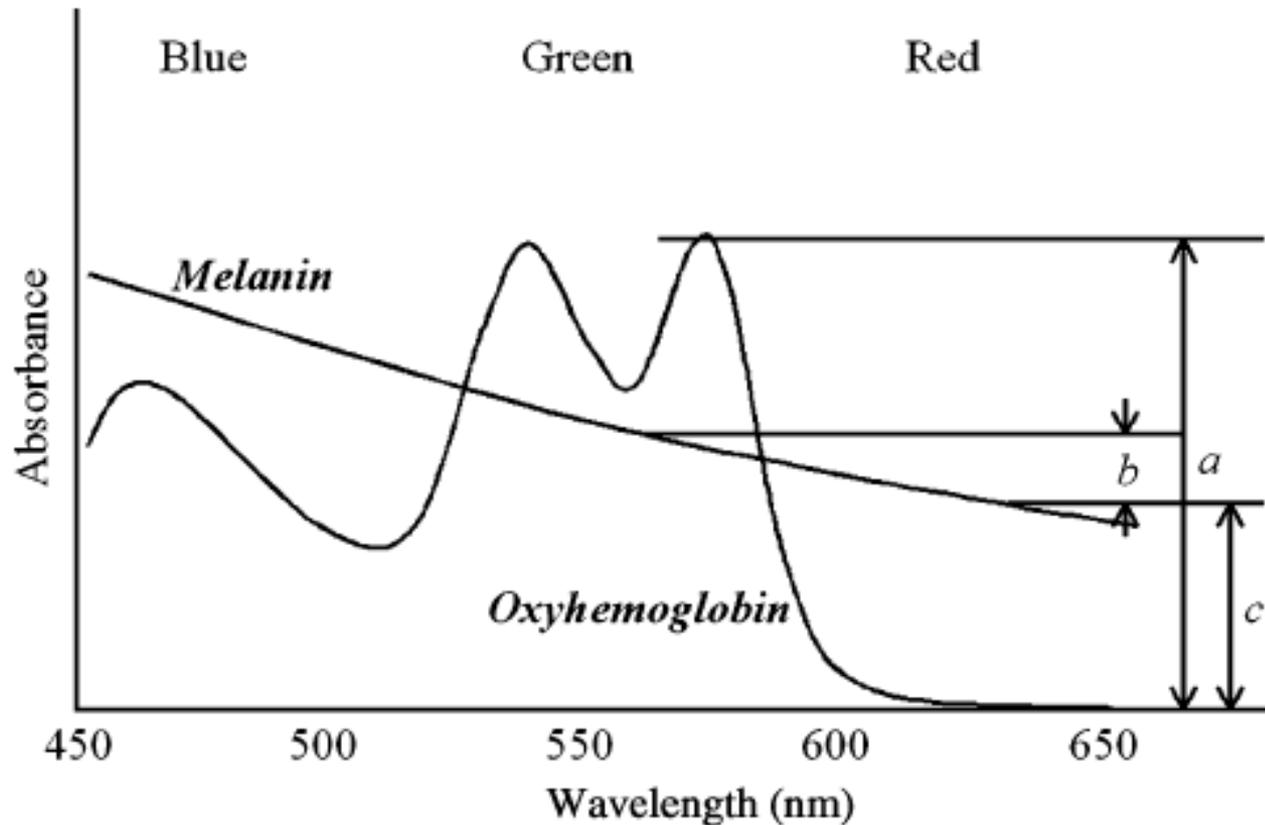


Fig. 2. Absorption spectra of melanin and hemoglobin and schematic conception of the erythema index (EI) and melanin index (MI) derived from images of the skin.

# Takiwaki's method based on absorbance spectra of multi-layered skin model

Assume two wavelength,  $\lambda_1$  and  $\lambda_2$ , equation (1) can be written as

$$A_1 - A_2 = (M_1 - M_2)C_m + (H_1 - H_2)C_h \quad (2)$$

In RGB color image,

for EI, 'green band' for  $\lambda_1$ , 'red band' for  $\lambda_2$  then,

$$A_1 - A_2 = \log(1 / R_{green}) - \log(1 / R_{red}) \quad (3)$$

for MI, 'red band' for both  $\lambda_1$  and  $\lambda_2$  then,

$$A = \log(1 / R_{red}) \quad (4)$$

# Kim's method based on HSV color space

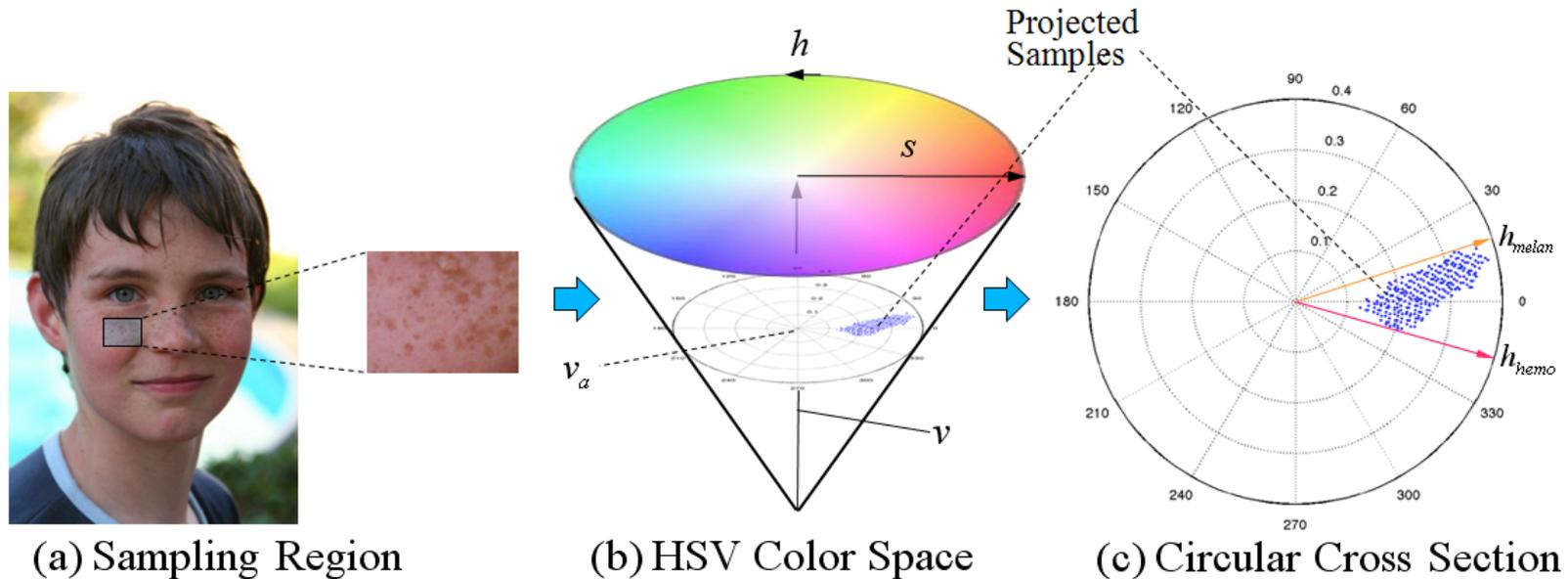


Fig. 3. (a) User-selected sampling region. (b) Circular cross section,  $(h, s, v_a)$ , computed by averaging brightness values of the sample. (c) Sample colors projected along the direction,  $(h_i, s_i, v_i)$  onto the circular cross section. Vector  $h_{melan}$ ,  $h_{hemo}$  represent 'melanin' and 'hemoglobin' respectively.

# Tsumura's method based on PCA and ICA

## Four assumptions as prerequisites:

- ◆ Lambert-Beer law holds is applicable in the skin layer for incident light
- ◆ spectral distribution of skin is not abrupt in sensitive spectral range of each channel in imaging system
- ◆ spatial variations of color in the skin are cause by two pigments: melanin and hemoglobin
- ◆ these quantities are mutually independent spatially



# Tsumura's method based on PCA and ICA

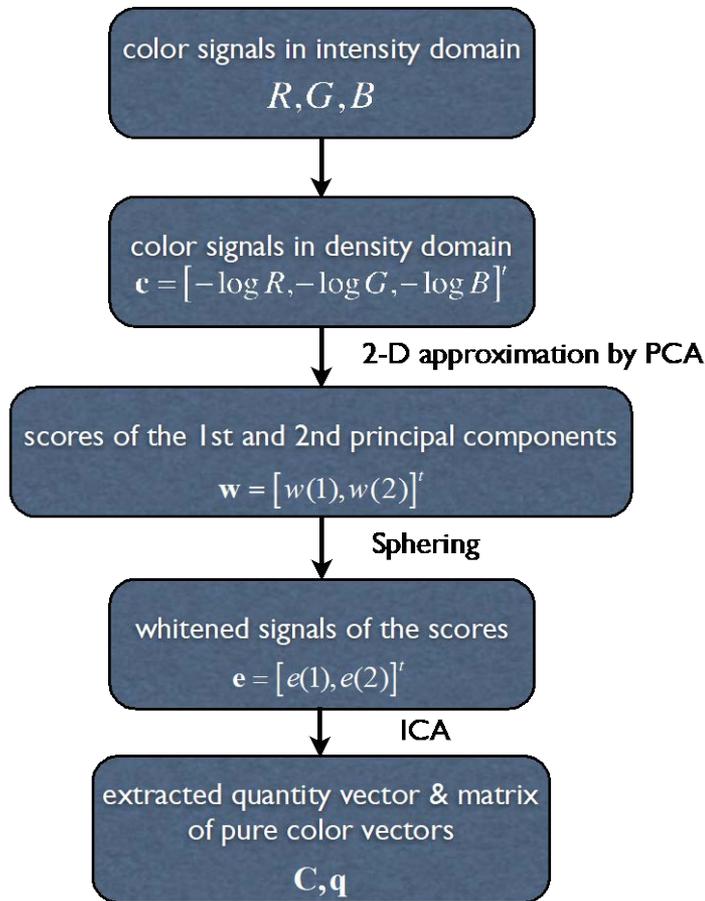


Fig. 4. Flowchart of preprocessing and ICA for a skin color image

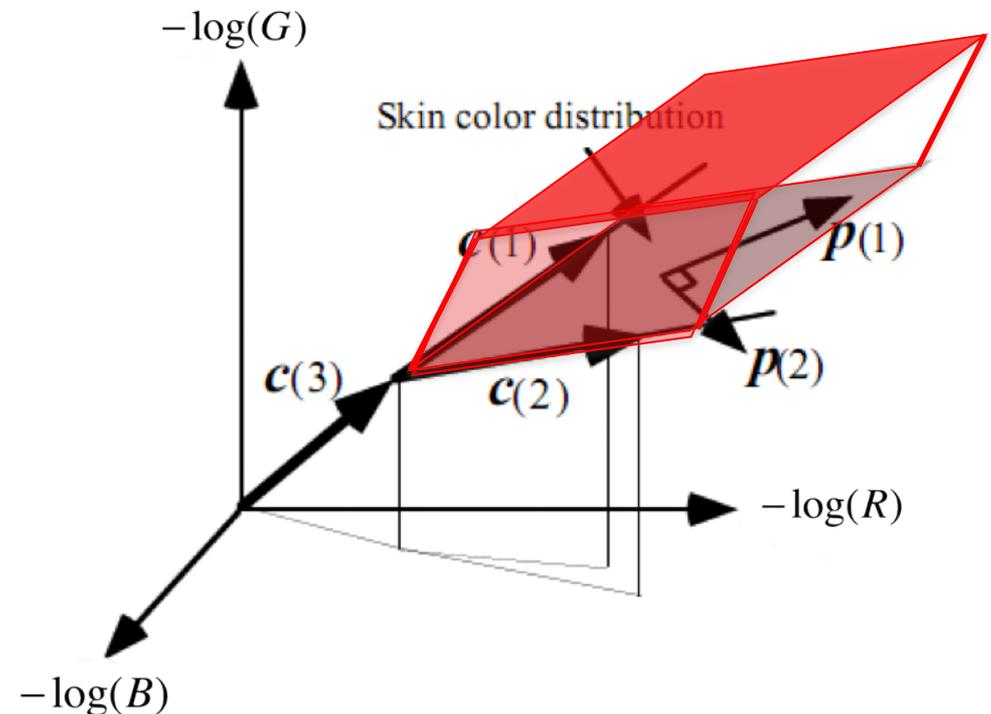


Fig. 5. Skin color model in the optical density domain

# New method based on Tsumura's approach

- Normalized RGB color space

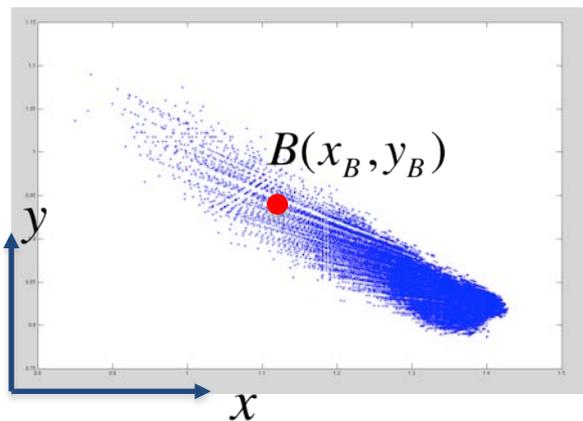
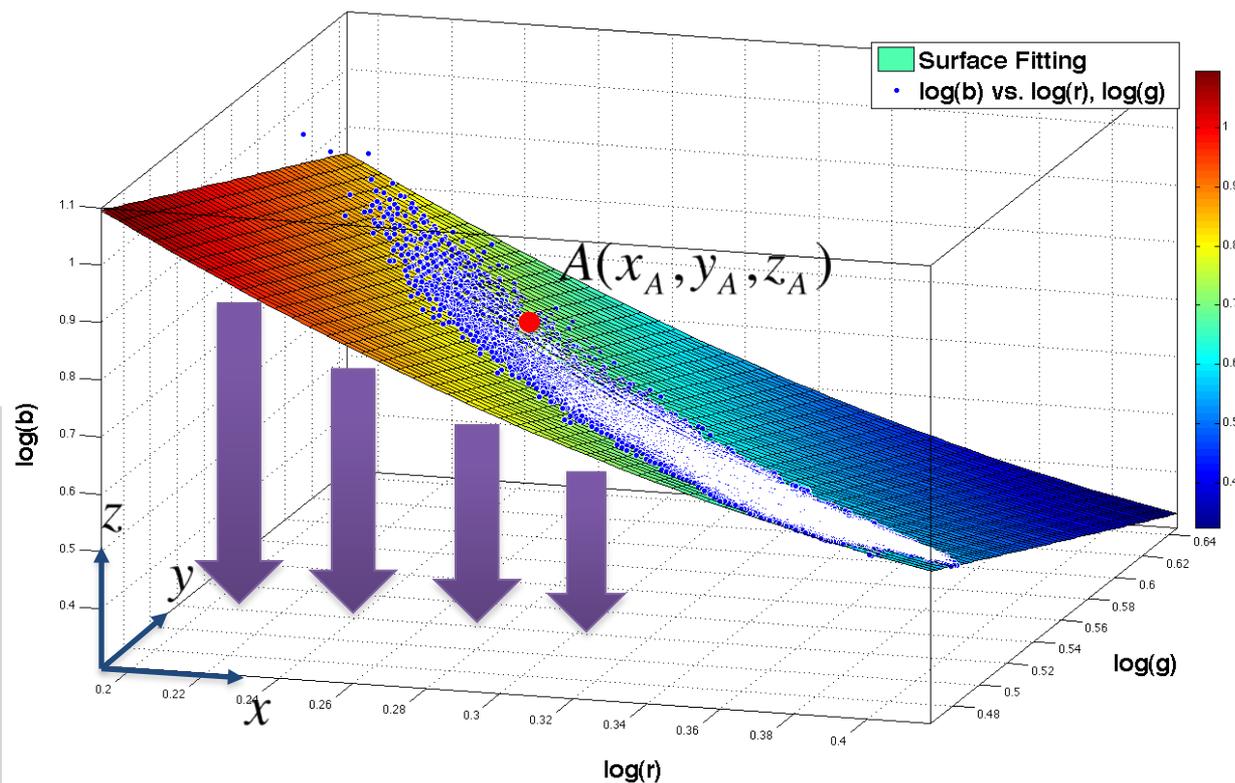
$$r = \frac{R}{R+B+G}, g = \frac{G}{R+B+G}, b = \frac{B}{R+G+B}$$

- Distribution in optical density domain

The distribution can be accurately described as a second order polynomial functions:

$$\log b = c_1 (\log r)^2 + c_2 (\log g)^2 + c_3 \log r + c_4 \log g + c_5$$

# New method based on Tsumura's approach



Flattened 2D plane



# New method based on Tsumura's approach

*Point*  $B(x_B, y_B)$  in the flatten 2D plane is a projection of *Point*  $A(x_A, y_A, z_A)$  in the 3D optical density space.

The coordinate transformation between  $A(x_A, y_A, z_A)$  and  $B(x_B, y_B)$  can be expressed as:

$$\begin{cases} x_B = \text{dist}_{\text{geodesic}}(A(x_A, y_A, z_A), P_1(0, y_A, c_2 y_A^2 + c_4 y_A + c_5)) \\ y_B = \text{dist}_{\text{geodesic}}(A(x_A, y_A, z_A), P_2(x_A, 0, c_1 x_A^2 + c_3 x_A + c_5)) \end{cases}$$





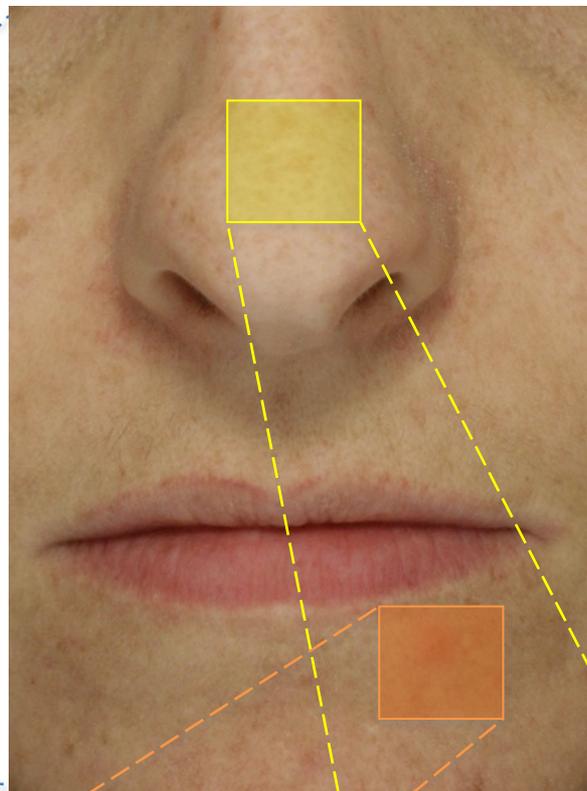
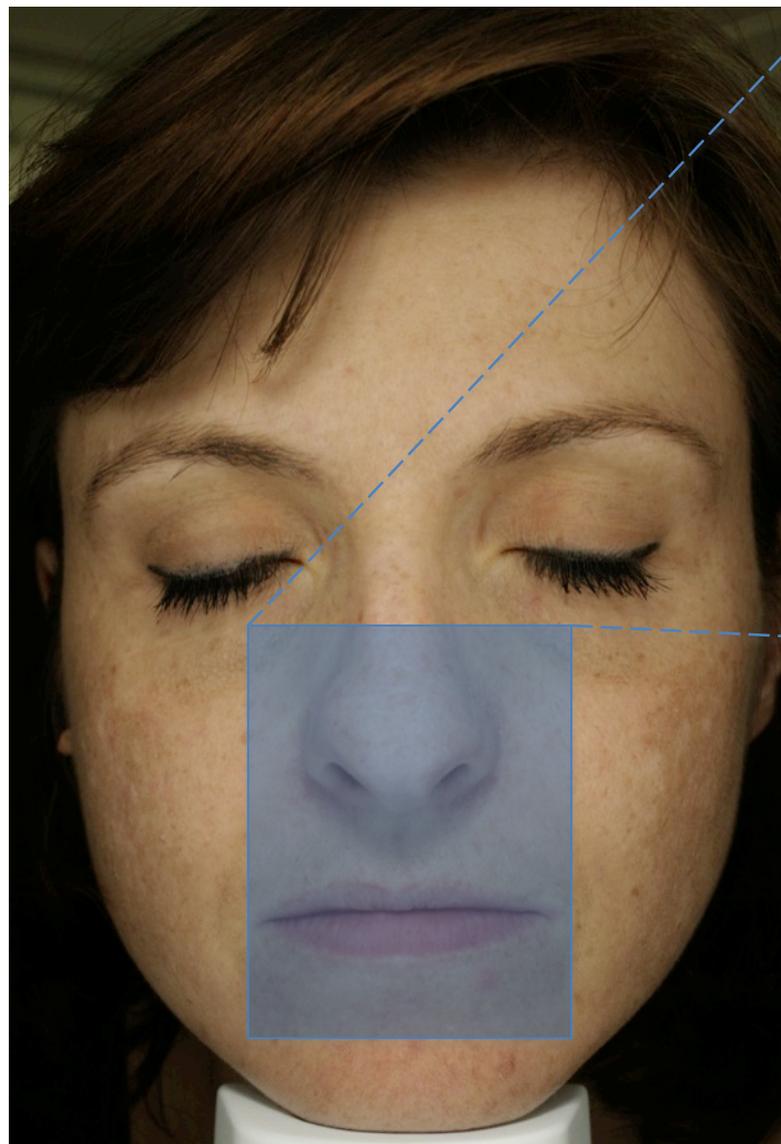
# Results and evaluation

RGB imaging based methods are useful in quantification on the perception of skin color, however, they provide relative index values rather than a standard (absolute measurements).

To evaluate the decomposition performs, we can refer to *pimple* and *freckle* as two physiological cues.



# Results and evaluation



Pimples



Freckles

# Results and evaluation



EI of Tsumura's method



EI of our method

# Results and evaluation



EI of Kim's method



EI of Takiwaki's method

# Results and evaluation

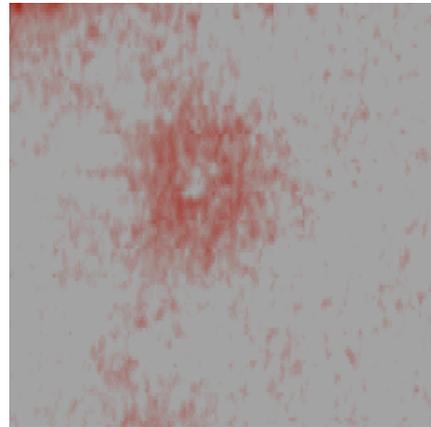


MI of Tsumura's  
method

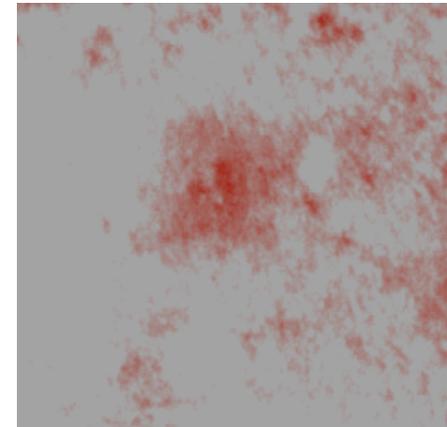


MI of our method

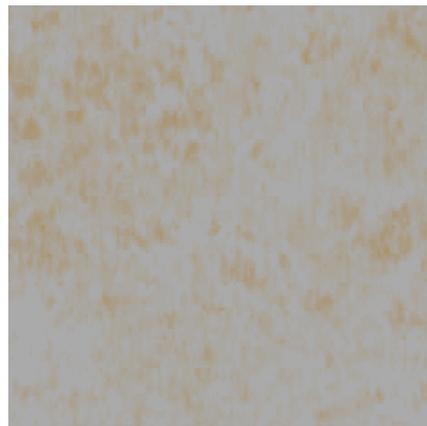
# Results and evaluation



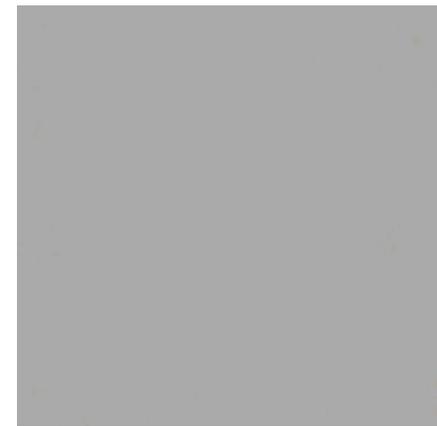
El of our method



El of Tsumura's method



MI of our method



MI of Tsumura's method

# Conclusion

Methods	Advantages	Disadvantages
Takiwaki's method	Ease of use; Objective assessment of intensity of pigmentation	Limited information; Possible artifacts
Kim's method	Relevant to color perception; Ease of use	Subjective results Possible artifacts
Tsumura's method	two-dimensional information	Small patches of ROIs only; Sensitive to shading effect
Our method	Invariant to illumination variation; Less sensitive to noise and shading effect	Limited information; Possible artifacts

# Perspective

Although we can approximate pigment quantity by using methods that rely on skin reflectance measured at a few selected wavelength bands, more accurate quantification can be achieved when we collect detailed spectral data.

In the future, we will use multi-spectral imaging based method.



THANK YOU!